

Deceived by the Fick principle: blood flow distribution in heart failure

Piergiuseppe Agostoni (1,2*, Gaia Cattadori^{2,3}, Carlo Vignati^{1,2}, Anna Apostolo (1, Stefania Farina¹, Elisabetta Salvioni¹, Silvia Di Marco³, Andrea Sonaglioni³, Savina Nodari⁴, Giancarlo Marenzi¹, Arno Schmidt-Trucksäss⁵, and Jonathan Myers⁶

¹Centro Cardiologico Monzino, IRCCS, Via Parea, 4, 20138 Milan, Italy; ²Department of Clinical Sciences and Community Health, Cardiovascular Section, University of Milano, Via Parea, 4, 20138 Milan, Italy; ³Multimedica IRCCS, Milan, Italy; ⁴Department of Medical and Surgical Specialities, Radiological Sciences and Public Health, University of Brescia Medical School, Brescia, Italy; ⁵Division of Sport and Exercise Medicine, Department of Sport, Exercise and Health, University of Basel, Birsstrasse 320B, CH-4052 Basel, Switzerland; and ⁶Cardiology Division, VA Palo Alto Health Care System and Stanford University, Palo Alto, CA, USA

Received 18 January 2024; revised 7 May 2024; accepted 6 June 2024; online publish-ahead-of-print 27 June 2024

See the editorial comment for this article 'Unravelling the complexities of exercise physiology in heart failure: begin with deconstructing the Fick principle', by E.H. Van Iterson, https://doi.org/10.1093/eurjpc/zwae268.

Aims	The Fick principle states that oxygen uptake (\dot{VO}_2) is cardiac output (Q_c) * arterial-venous O_2 content difference [$\Delta C(a-v) O_2$]. Blood flow distribution is hidden in Fick principle, and its relevance during exercise in heart failure (HF) is undefined. To highlight the role of blood flow distribution, we evaluated peak exercise \dot{VO}_2 , Q_c , and $\Delta C(a-v)O_2$, before and after HF therapeutic interventions.
Methods and results	Symptom-limited cardiopulmonary exercise tests with Q_c measurement (inert gas rebreathing) was performed in 234 HF patients before and 6 months after successful exercise training, cardiac resynchronization therapy, or percutaneous edge-to-edge mitral valve repair. Considering all tests ($n = 468$), a direct correlation between peak $\dot{V}O_2$ and peak Q_c ($R^2 = 0.47$) and workload ($R^2 = 0.70$) was observed. Patients were grouped according to treatment efficacy in Group 1 (peak $\dot{V}O_2$ increase >10%, $n = 93$), Group 2 (peak $\dot{V}O_2$ change between 0 and 10%, $n = 60$), and Group 3 (reduction in peak $\dot{V}O_2$, $n = 81$). Post-treatment peak $\dot{V}O_2$ changes poorly correlated with peak Q_c and peak $\Delta C(a-v)O_2$ changes. Differently, post-procedure peak Q_c vs. peak $\Delta C(a-v)O_2$ changes showed a close negative correlation ($R^2 = 0.46$), becoming stronger grouping patients according to peak $\dot{V}O_2$ improvement ($R^2 = 0.64$, 0.79, and 0.58 in Groups 1, 2, and 3, respectively). In 76% of patients, peak Q_c and $\Delta C(a-v)O_2$ changes diverged regardless of treatment.
Conclusion	The bulk of these data suggests that blood flow distribution plays a pivotal role on peak $\dot{V}O_2$ determination regardless of HF treatment strategies. Accordingly, for assessing HF treatment efficacy on exercise performance, the sole peak $\dot{V}O_2$ may be deceptive and the combination of $\dot{V}O_2$, Q_c and $\Delta C(a-v)O_2$, must be considered.
Lay summary	This study aimed to understand how oxygen uptake during exercise is affected by heart failure therapeutic intervention. We evaluated 234 heart failure patients before and after treatments such as exercise training, cardiac resynchronization therapy, or mitral valve repair, finding that changes in oxygen uptake were poorly correlated with changes in cardiac output and oxygen content difference between arteries and veins. However, we observed a strong negative correlation between changes in cardiac output and oxygen uptake during exercise, regardless of treatment. Therefore, relying solely on oxygen uptake may not accurately assess treatment effectiveness, and considering a combination of oxygen uptake, cardiac output, and oxygen content difference is important.
Keywords	Peak \dot{VO}_2 • Blood flow distribution • Heart failure • Fick principle

* Corresponding author. Tel: +39 2 58002772, Email: piergiuseppe.agostoni@ccfm.it

 $\ensuremath{\mathbb{C}}$ The Author(s) 2024. Published by Oxford University Press on behalf of the European Society of Cardiology.

This is an Open Access article distributed under the terms of the Creative Commons Attribution-NonCommercial License (https://creativecommons.org/licenses/by-nc/4.0/), which permits non-commercial re-use, distribution, and reproduction in any medium, provided the original work is properly cited. For commercial re-use, please contact reprints@oup.com for reprints and translation rights for reprints. All other permissions can be obtained through our RightsLink service via the Permissions link on the article page on our site—for further information please contact journals.permissions@oup.com.

Key findings

- Oxygen uptake during exercise was strongly related to cardiac output and workload.
- Changes in cardiac output and oxygen content difference were closely related after treatments, especially in patients with significant improvement in oxygen uptake.

Introduction

The Fick principle states that oxygen uptake $(\dot{V}O_2)$ is equal to cardiac output (Q_c) * arterial-venous O₂ content difference $[\Delta C(a-v)O_2]$. Consequently, for the same $\dot{V}O_2$, if Q_c increases, $\Delta C(a-v)O_2$ reduces, and vice versa, if Q_c reduces, $\Delta C(a-v)Q_2$ increases. Q_c is cardiac function and $\Delta C(a-v)O_2$ has been used as a metric to reflect the muscle capacity to extract O_2 .^{2–7} However, evidence suggests that changes in Q_c and $\Delta C(a-v)O_2$ do not completely reflect changes in VO₂.^{4,8,9} As a matter of fact, \dot{VO}_2 is directly related to Q_c , lung function, and haemoglobin level, as well as diffusion capacity of O_2 from the capillaries to the mito-chondria and to muscle performance.^{3,9,10} In the Fick principle, the concept of distribution of blood flow is hidden. This is a relevant issue in normal subjects since during exercise, blood flow to the working muscle increases more than total blood flow.⁹ Differently in heart failure (HF), maladaptive vasoconstrictor control mechanisms prevent redistribution of blood flow from non-working muscles, kidney, gut, and liver to working muscles.^{11,12} This is relevant even at rest, where VO_2 progressively reduces as HF severity increases, so VO₂ needs to be measured and cannot be estimated by any prediction formula.^{13,14} Moreover, during exercise, distribution of blood flow is difficult to be measured and only indirect data are available to support its role.^{9,15} In an attempt to analyse the presence and relevance of blood flow distribution during exercise, we evaluated the three components of the Fick principle, $\dot{V}O_2$, Q_c , and $\Delta C(a-v)O_2$, during exercise before and after a clinical HF intervention aimed at improving exercise through different mechanisms. These included cardio-respiratory exercise training, cardiac resynchronization therapy (CRT), and percutaneous edge-to-edge mitral valve repair (pMVR). Indeed, purported primary effects of exercise training are blood flow increase and oxygen extraction by the muscles, of CRT is Q_c increase, and of pMVR are Q_c increase and capillary pulmonary pressure reduction, respectively.^{16–18}

In brief, the purpose of the present study was to evaluate whether blood flow redistribution during exercise is affected by different interventions aimed at improving HF status.

Methods

Study population

We evaluated the results from HF patients regularly followed at HF Unit of Centro Cardiologico Monzino Milan enrolled in three different treatment protocols concerning haemodynamic effects of exercise training, CRT, and pMVR reported in previous publications.^{8,19,20} Of note, the exercise training study included patients evaluated at Inselspital, Bern University Hospital, Bern, Switzerland. All patients had been familiarized with cardiopulmonary exercise testing (CPET). Study inclusion criteria were HF due to ischaemic or dilated cardiomyopathy, stable clinical conditions, New York Heart Association (NYHA) class II or III, optimal HF treatment, and capability of performing CPET with Q_c determination by inert gas rebreathing (IGR) method.^{21,22} Further inclusion criteria were applied for each protocol, specifically left ventricular ejection fraction (LVEF) < 40% for the exercise training protocol,⁸ the presence of the protocol-specific criteria for CRT selection,²⁰ and clinical indication according to guidelines for CRT and pMVR protocols,¹⁹ respectively.

Study exclusion criteria were any comorbidities directly affecting exercise performance, planned cardiovascular or extra-cardiac procedures, and significant pulmonary dysfunction.

In each study, HF patients who meet the study inclusion/exclusion criteria were asked to participate to the different studies and eventually recruited consecutively. Of note, the three studies were done at different times being exercise training the oldest study, CRT intermediate, and pMVR the most recent one. Each study complied with the Declaration of Helsinki, the locally appointed Scientific and Ethics Committees approved all the research protocols, and informed consent was obtained from all patients. The present analysis of data was approved by the local Ethics Committee (CCM1896). Of note, the present was a retrospective analysis of data obtained by three independent prospective studies. The analysis plan was developed in advance and built knowing the results of each original study except for the analysis of different groups based on peak VO₂ changes, which was done *a posteriori*.^{8,19,20}

Study design Pre-treatment evaluation

All patients received a careful clinical evaluation including clinical history and recent instrumental data to confirm treatment selection. All subjects underwent an electrocardiogram, a standard echocardiogram, a CPET (cycle ergometer) for familiarization purposes, and at least one teaching session to familiarize subjects with IGR methodology. Finally, a CPET based on a personalized ramp protocol aimed at achieving maximal effort was performed along with Q_c measurement by IGR at rest and at peak exercise. $\Delta C(a-v)O_2$ was calculated following the Fick principle as $\Delta C(a-v)O_2 = \dot{V}O_2/Q_c$.

Post-treatment evaluation

At the end of the rehabilitation programme and after at least 6 months of follow-up in case of CRT and pMVR, patients underwent clinical and instrumental evaluation, including a CPET with Q_c measurement and using the same ramp workload protocol as in the pre-treatment study. Of note, patients who underwent CRT or pMVR were not enrolled in any rehabilitation programme.

Echocardiography

Standard 2D, colour, and spectral Doppler measurements were performed. Left ventricular ejection fraction was determined using the Simpson rule algorithm by tracing the left ventricular 2D area in standard apical two- and four-chamber views at end-systole and end-diastole.

Cardiopulmonary exercise testing

Cardiopulmonary exercise testing was performed on a cycle ergometer with progressive work rate increase in a ramp pattern, after 3 min of rest and 3 min of unloaded cycling. Expired O_2 , carbon dioxide (CO₂), and ventilation were measured breath by breath (Innocor® rebreathing system, Innovision A/S, Odense, Denmark). A 12-lead electrocardiogram was recorded continuously during the test (Marquette, Case800, Milwaukee, WI). Patients were strongly encouraged to perform a maximal test, allowing the final 30 s for the rebreathing manoeuvre. The work rate increase during the test was individualized to achieve peak exercise in 8–10 min during the increasing work rate period.²³ The CPET was interpreted and reported as previously outlined in detail.²⁴ Peak \dot{VO}_2 values were averaged over 20 s.

Q_c measurement

Non-invasive $Q_{\rm c}$ measurements were performed during CPET at rest and at peak exercise using the Innocor rebreathing system. 22 The IGR technique has been previously described in detail. 21 In brief, IGR uses an oxygenenriched mixture of an inert soluble gas [0.5% nitrous oxide (N₂O)] and an inert insoluble gas [0.1% sulfur hexafluoride (SF₆)] from a pre-filled bag. Patients breathed into a respiratory valve via a mouthpiece and a bacterial filter with a nose clip. At the end of the expiration, the valve is activated, so that the patient re-breathes from the pre-filled bag for a period of 10–20 s. After this period, the patient is switched back to ambient air, and the $Q_{\rm c}$ measurement is terminated. Photo-acoustic analysers measure gas concentration over a five-breath interval. SF₆ is insoluble in blood, and it is used to determine lung volume. N₂O is soluble in blood, and its

2	n	n	Э
4	υ	υ	Э

	Entire population, <i>n</i> = 234	Exercise training, <i>n</i> = 70	CRT, <i>n</i> = 93	pMVR, <i>n</i> = 71	Р
Age (years)	68 ± 11	62 <u>±</u> 10	67 <u>+</u> 10	75 ± 9	<0.01
Sex (male/female)	182/52	54/16	77/16	51/20	0.28
Heart failure aetiology (ischaemic/not ischaemic)	124/110	37/33	56/37	31/40	ns
NYHA class	2.4 ± 0.6	2.0 ± 0.5	2.5 ± 0.5	2.5 ± 0.6	<0.01
EDV (mL)	193 <u>+</u> 73	192 ± 76	212 <u>+</u> 69	168 <u>+</u> 68	<0.01
ESV (mL)	129 ± 67	135 ± 70	150 <u>+</u> 60	93 <u>+</u> 58	<0.01
LVEF (%)	34 ± 12	32 <u>±</u> 10	28 ± 6	46 <u>+</u> 13	<0.01
ACEi/ARB/ARNI	85%	93%	89%	77%	<0.01
Beta-blockers	80%	96%	83%	62%	<0.01
Loop diuretic	79%	80%	81%	77%	<0.01
MRA	45%	57%	38%	39%	<0.01
Antiplatelet therapy	57%	57%	62%	52%	ns
Oral anticoagulant	33%	40%	26%	33%	ns
Digoxin	6%	7%	2%	10%	ns
Amiodarone	34%	29%	43%	30%	ns

Table 1 Pre-intervention characteristics of the entire population and according to the three procedures undertaken

CRT, cardiac resynchronization therapy; pMVR, percutaneous mitral valve repair; NYHA, New York Heart Association; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; ACEi, angiotensin-converting enzyme inhibitor; ARB, angiotensin receptor blocker; ARNI, angiotensin receptor-neprilysin inhibitor; MRA, mineralocorticoid receptor antagonist; ns, not significant.

concentration decreases during rebreathing with a rate proportional to pulmonary blood flow (PBF), which is the blood flow that perfuses the part of the alveoli where gas exchange takes place. Q_c is equal to PBF when the arterial oxygen saturation measure (SpO₂) is high (>98% using the pulse oximeter). In a case of minor desaturation, shunt flow estimation is added to PBF to calculate Q_c . Differently, in the case of SpO₂ \leq 90%, the estimation of shunt flow became questionable and Q_c measurement by IGR unreliable.

Statistical analysis

Continuous variables are presented as mean \pm standard deviation (SD). When the distribution was not normal, variables were log-transformed to allow homogeneous comparisons. Differences between before and after treatment were evaluated by paired *t*-test. Differences between multiple groups were assessed by repeated measures analysis of variance, accounting for both between-group and within-group differences, followed by Bonferroni *post hoc* correction. Correlation coefficients between the three components of the Fick principle were assessed by best fit method. All tests were two sided. A *P* < 0.05 was considered statistically significant. Analyses were performed using IBM SPSS statistics 27.

Results

We studied 273 HF patients who were treated with one of the following interventions: pMVR, CRT, and exercise training. Thirty-nine patients did not perform the 6-month evaluation due to death or inability to exercise (3 cases each); cerebral stroke, pMVR failure, or peak exercise measurement failure were reported in 2 cases each; lung cancer, aortic aneurism, and atrial fibrillation (CRT group) were reported in 1 patient each; and 24 patients withdrew informed consent or were lost to follow-up. The remaining 234 patients were included in the present analysis. Of these, 71 underwent pMVR, 93 CRT, and 70 exercise training. *Table 1* reports demographic data, HF aetiology, NYHA class, cardiac ultrasound data, and therapy before intervention for the entire study population and according to treatment.

Major resting and peak exercise cardiorespiratory data of the entire population and of the three clinical interventions are reported in *Table 2*.

The best fit correlation between $\dot{V}O_2$ vs. Q_c and $\dot{V}O_2$ vs. workload at peak exercise in the entire population, both before and after treatments, is reported in *Figure 1A* and *B*, respectively. We confirmed the close correlation between peak $\dot{V}O_2$ and Q_c and peak workload.

Patients were grouped according to treatment efficacy in Group 1 (peak $\dot{V}O_2$ increase >10%), Group 2 (peak $\dot{V}O_2$ change between 0 and 10%), and Group 3 (reduction in peak VO_2 with treatment). In parallel with peak $\dot{V}O_2$ changes, changes in peak workload and peak Q_c were observed (*Table 3*).

A correlation between post-procedure–pre-procedure peak $\dot{V}O_2$ vs. post-procedure–pre-procedure peak workload ($R^2 = 0.226$) was observed in the entire study population (see Supplementary material online, *Figure S1*). Similar correlations were observed when exercise training, CRT, and pMVR were considered separately: exercise training $R^2 = 0.19$, CRT $R^2 = 0.24$, and pMVR $R^2 = 0.26$.

In terms of the effect of treatments on changes in Fick variables between post-procedure–pre-procedure peak \dot{VO}_2 vs. peak Q_c , the relationship was poor across the entire population (*Figure 2A*) as was the correlation between post-procedure and pre-procedure peak \dot{VO}_2 vs. peak $\Delta C(a-v)O_2$ (*Figure 2B*). However, following the different haemodynamic actions of the three treatments, some differences were observed; specifically, the peak \dot{VO}_2 vs. peak Q_c correlation was $R^2 = 0.02$, $R^2 = 0.27$, and $R^2 = 0.16$ for exercise training, CRT, and pMVR, respectively. As regards post-procedure—pre procedure peak \dot{VO}_2 vs. peak $\Delta C(a-v)O_2$, the correlation was $R^2 = 0.04$, $R^2 = 0.25$, and $R^2 = 0.37$ for exercise training, CRT, and pMVR, respectively.

The post-procedure–pre-procedure changes in peak exercise Q_c vs. $\Delta C(a-v)O_2$ showed a close negative correlation in the entire study population ($R^2 = 0.46$; *Figure 3A*). This correlation became stronger when separately considering patients who improved peak $\dot{V}O_2$ by >10% (Group 1, $R^2 = 0.64$), patients who changed peak $\dot{V}O_2$ between 0 and 10% (Group 2, $R^2 = 0.79$), and patients who showed a reduction in peak $\dot{V}O_2$ (Group 3, $R^2 = 0.58$; *Figure 3B* and *Table 3*). The correlation was progressively shifted upwards and rightwards from Group 3 to Group 1. Considering different treatment strategies separately, the post-procedure–pre-procedure changes in peak exercise Q_c vs. $\Delta C(a-v)O_2$ were $R^2 = 0.68$, 0.22, and 0.20 for exercise training, CRT,

	Total	n = 234	Exercise tr.	aining <i>n</i> = 70	CRT	n = 93	PMVF	₹ n = 71	
	Pre	Post	Pre	Post	Pre	Post	Pre	Post	ď
Rest VO ₂ (mL/min)	309 ± 87	307 ± 69 ^{NS}	337 ± 108	312 土 74 ^{NS}	301 ± 82	312 土 70 ^{NS}	294 ± 62	294 土 59 ^{NS}	0.460
Rest HR (b.p.m.) ^a	71 ± 13	$69 \pm 13^{*}$	75 ± 15	73 ± 15^{NS}	67 ± 12	66 ± 10^{NS}	71 ± 12	69 ± 12^{NS}	0.016
Rest Q _c (L/min) ^a	3.3 ± 1.0	$3.5\pm\mathbf{1.0*}$	3.7 ± 1.1	3.9 ± 1.1^{NS}	3.2 ± 1.0	3.4 ± 0.9^{NS}	3.1 ± 0.8	3.3 ± 0.8^{NS}	0.005
Rest $\Delta C(a-v)O_2 (mL/100 mL)^a$	9.9 ± 3.6	9.3 ± 2.8^{NS}	$\textbf{9.8} \pm \textbf{4.3}$	$8.6 \pm 2.6^{*}$	9.9 ± 3.5	9.8 ± 3.0 ^{NS}	10 ± 2.9	9.4 ± 2.5^{NS}	0.065
Hb (g/dL)	13.6 ± 1.6	13.3 ± 1.5^{NS}	13.6 ± 1.7	13.3 ± 2^{NS}	13.3 ± 1.4	13.1 ± 1.4^{NS}	13.7 ± 1.7	13.6 ± 1.6^{NS}	0.141
Peak workload (Watt) ^a	63 ± 27	$67\pm29^{*}$	69 ± 29	$73 \pm 32^{*}$	67 ± 30	$70 \pm 30^{*}$	54 ± 18	56 ± 19^{NS}	<0.001
Peak ՝O2 (mL/min)	$\textbf{1023} \pm \textbf{351}$	$1089 \pm \mathbf{384*}$	1111 ± 403	$1191 \pm 441^*$	$\textbf{1067}\pm\textbf{357}$	$1156 \pm 377*$	875 ± 226	897 ± 244 ^{NS}	<0.001
Peak ḋO2/kg (mL/kg/min)	13.5 ± 3.9	$14.3 \pm 4.5 \ast$	14.1 ± 3.9	$\textbf{15.1} \pm \textbf{4.6}^{*}$	$\textbf{13.8} \pm \textbf{3.8}$	$14.9 \pm 4.6^{*}$	12.4 ± 3.7	12.4 ± 4.2 ^{NS}	<0.001
Peak HR (b.p.m.) ^a	104 ± 22	102 ± 21^{NS}	110 ± 23	108 ± 23^{NS}	$\textbf{102} \pm \textbf{20}$	$98\pm18^{*}$	100 ± 23	100 ± 20^{NS}	0.146
Peak Q _c (L/min) ^a	6.1 ± 1.9	$\textbf{6.9} \pm \textbf{2.2*}$	6.6 ± 2.2	$7.3 \pm 2.5^{\circ}$	$\textbf{6.2} \pm \textbf{1.8}$	$7.0 \pm 2.2^{*}$	5.6 ± 1.5	$6.3 \pm 1.6^{*}$	<0.001
Peak C(a-v)O ₂ (mL/100 m) ^a	$\textbf{17.0} \pm \textbf{4.1}$	$\textbf{16.3} \pm \textbf{4.6}^{*}$	17.5 ± 5.1	16.6 ± 4.1^{NS}	17.1 ± 3.0	16.7 ± 2.9^{NS}	$\textbf{16.3} \pm \textbf{4.0}$	$14.7 \pm 3.8^*$	0.002
Peak RER	1.05 ± 0.11	$1.05 \pm 0.10^{\rm NS}$	1.04 ± 0.08	1.04 ± 0.08^{NS}	1.06 ± 0.12	1.05 ± 0.11^{NS}	1.04 ± 0.11	1.05 ± 0.11^{NS}	0.752
ừO₂ AT (mL/min)	$\textbf{740} \pm \textbf{202}$	$795\pm240^{*}$	723 ± 167	$784 \pm 222^{*}$	802 ± 231	$864 \pm 270^{*}$	676 ± 167	$703 \pm 171*$	0.003
VE/VCO₂ slope	35 ± 8	34 ± 8^{NS}	32 ± 7	33 ± 7^{NS}	37 ± 8	$35 \pm 10^{*}$	35 ± 7	35 ± 7^{NS}	0.344

NS: (post vs. pre) not significant: ** (post vs. pre) P < 0.05. ^aNon-normally distributed variables were log transformed and compared by t-test. Bold identifies statistical significant comparisons. ^bANOVA repeated measures.

P. Agostoni et al.





and pMVR, respectively (see Supplementary material online, Figure S2A–C). Haemodynamic data of the entire study population are reported according to the quadrant (Figure 3A). Of note, the greatest peak $\dot{V}O_2$ and workload increases were observed in patients belonging to the right upper quadrant, but the greatest Q_c increase was observed in those in the right lower quadrant. Indeed, post-procedure–pre-procedure changes between Q_c vs. $\Delta C(a-v)O_2$ were consensual in 24% of cases in the entire study population and in 16, 28, and 27% of cases in exercise training, CRT, and pMVR groups, respectively.

Discussion

The present study, applying consolidated parameters of exercise haemodynamic pre- and post-different therapeutic interventions, confirms a pivotal role of blood flow distribution on exercise performance in HF patients.²⁵ Indeed, the Fick formula is based on the conservation

of mass principle and report the correlation between VO₂, Q_c, and $\Delta C(a-v)O_2$ and, per se, is not misleading as suggested, provocatively, in the present report title. However, misleading may be its arbitrary application on the effect of exercise on changes of Fick generating parameters. Indeed, changes in VO₂ after any intervention may be due to changes in Q_c and/or $\Delta C(a-v)O_2$ that may be in parallel or not so that VO₂ may not be assumed as always and fully indicative of the results of an intervention.

We measured resting and exercise Q_c by IGR, which is a reliable technique in patients without cardiac disease or significant intrapulmonary shunt.²¹ Indeed, a few previous studies demonstrated the reliability of IGR Q_c measurements during exercise.^{26,27} However, several studies reported that Q_c measure by IGR is reliable even in this condition and does not alter main cardiopulmonary parameters.^{26,28} Nonetheless, IGR requires patient's collaboration and instruction. Accordingly, several IGR familiarization sessions were completed before the study. The use of familiarization sessions resulted in only

	Group 1 (∆peakVO₂ > 10%), n = 93	Group 2 (∆peakVO₂ 0–10%), n = 60	Group 3 (∆peakVO₂ < 0), n = 81	Р
ΔPost–pre peak VO ₂ (%)	28 ± 16*°	4 ± 4°^	-13 ± 13*^	<0.001
$\Delta Post-pre peak Q_c (\%)^a$	29 ± 34*°	10 ± 36^	5 ± 23^	<0.001
$\Delta Post-pre peak \Delta C(a-v)O_2 (\%)^a$	$5 \pm 32^{\circ}$	$5 \pm 36^{\circ}$	-13 ± 22*^	<0.001
$\Delta Post-pre peak workload (%)^a$	19 <u>+</u> 24*°	8±13°^	-4 ± 16*^	<0.001
Pre-treatment peak \dot{VO}_2 (mL/min)	12.7 ± 3.6°	13.5 ± 4	14.4 <u>+</u> 3.8	0.002
Pre-treatment peak Q _c (L/min) ^a	5.9 ± 1.8	6.4 ± 2	6.1 ± 1.8	ns
Pre-treatment peak $C(a-v)O_2(mL/100 mL)^a$	16.5 <u>+</u> 4	17 <u>+</u> 4.4	17.7 <u>+</u> 3.9	ns
Pre-treatment peak workload (watt) ^a	62 ± 27	67 <u>±</u> 27	63 <u>+</u> 27	ns

Table 3	Differences in	patients gro	uped according	g to treatment efficad	cy (∆peakVO ₂)
---------	----------------	--------------	----------------	------------------------	----------------------------

 VO_2 , oxygen consumption; Q_c , cardiac output; $\Delta C(a-v)O_2$, arterial-venous oxygen difference; $\dot{V}O_2$, oxygen uptake; ns, not significant.

°P < 0.001 vs. Group 3; *P < 0.001 vs. Group 2; ^P < 0.001 vs. Group 1.

^aNon-normally distributed variables.

rare failure of IGR at peak exercise, which occurred in only in two cases. As regards IGR technique, it must be acknowledge that a limited misalignment between peak exercise VO₂ and Q_c measures exists. We used VO₂ data collected in the 20 s preceding the IGR technique that lasted up to 10 s so that the error added by signal misalignment, if any, is really minor.

The presence of blood flow redistribution during exercise has been suggested for many years but it has been thought to be more of a 'dogma', in part because it is difficult to quantify. Indeed, it has been suggested that to optimally redistribute blood flow during exercise, there must be vasodilation to areas in need, such as skeletal muscle, and sympathetically mediated vasoconstriction to non-exercising areas, such as viscera and adipose tissue. Among the evidence of variable blood flow distribution in HF are data comparing O_2 content in the femoral vein (CfvO₂) and pulmonary artery (CpaO₂) and data comparing leg blood flow vs. Q_c . These studies have shown that CpaO₂ and leg blood flow were closer to $CfvO_2$ and Q, respectively, the greater the severity of HF.²⁹⁻³⁵ These data were suggestive of redistribution of blood flow towards the exercising muscle so that the percentage of Q_c towards the working muscle was greater the greater the HF severity. However, these studies are challenging to perform and are invasive, requiring simultaneous femoral vein blood flow and Q_c measurements or pulmonary artery, femoral vein, and systemic artery sampling during exercise.^{29,34–36} Thus, there have been a very limited number of such studies with very few patients as well as some uncertainness regarding the reliability of the measurements. The current study extends these previous efforts in that it is based on a sizable number of patients and applied consolidated techniques. Indeed, we used post- vs. preprocedural exercise changes of Fick principle parameters to bring greater clarity to changes in blood flow distribution.

According to Sir Joseph Barcroft,³⁷ the condition of exercise is not a mere variant of the condition of rest, it is the essence of the machine. At peak exercise, $\dot{V}O_2$ was strongly correlated with both Q_c and workload (*Figure 1A* and *B*). The $\dot{V}O_2$ vs. workload relationship had a $R^2 = 0.4707$, which is suggestive of a role of both central and peripheral mechanisms in the determination of peak $\dot{V}O_2$. Also peak $\dot{V}O_2$, peak Q_c , and peak $\Delta C(a-v)O_2$ changes with treatment offer minimal insight on blood flow distribution (*Table 2*). As a matter of fact, a peak $\dot{V}O_2$ increase should be associated with an increase in peak $\Delta C(a-v)O_2$. However, in a few patients, albeit a relevant peak Q_c increase, peak $\Delta C(a-v)O_2$ reduces (*Figure 3A* and *B*), and consequently, peak $\dot{V}O_2$ increase is blunted. Accordingly, something else may be occurring not well demonstrated by the Fick principle as suggested by the

correlation between peakVO₂ changes and workload changes after treatments (see Supplementary material online, *Figure S1*), which showed that only about 23% of peak workload increase was related to peakVO₂. That means that the 77% of peak workload changes could not be attributed directly to peakVO₂ changes. Notably, this was observed irrespective of the treatment strategies adopted that act primary on different haemodynamic and non-haemodynamic functions associated with exercise performance. Overall, these data cannot precisely identify blood flow distribution differences during exercise, but they provide surrogates to support our hypothesis that differences in blood flow distribution have an important impact on exercise tolerance.

Patients may improve peak VO2 with treatment by different combinations of changes in peakQ_c and peak $\Delta C(a-v)O_2$. Of note, among patients who undergo interventions, those who simultaneously improved or reduced both peakQ_c and peak $\Delta C(a-v)O_2$ were a minority, representing 18 and 6% of cases, respectively. Thus, in 76% of the cases, changes in peakQ_c and peak $\Delta C(a-v)O_2$ diverged, so that exercise flood flow distribution likely changed between pre- and post-treatment conditions. The post-procedure-pre-procedure changes in peak exercise Q_c vs. $\Delta C(a-v)O_2$ diagram (*Figure 3A*) showed a negative slope, which implied blood flow distribution changes with therapy, while a positive slope argued against a relevant redistribution. Figure 3A shows that patients belonging to the right upper quadrant were those with the greatest peak $\dot{V}O_2$ increase but not those with the greatest peak Q_c increase who were in the lower right panel. Moreover, grouping patients according to their peakVO2 increase (Figure 3B), the post-procedurepre-procedure changes in peakQ_c vs. $\Delta C(a-v)O_2$ slope shifted upwards and to the right, but the inclination of the slope was maintained, suggesting the presence of the blood flow redistribution regardless of the efficacy of treatment in terms of peak \dot{VO}_2 increase. Of note, the correlations observed for each of the HF subgroups were stronger than the correlation obtained considering the entire population. It must be underlined that $\Delta C(a-v)O_2$ is influenced by several factors on top of blood flow distribution including perfusion and diffusion of O_2 , as well as O_2 demand by the mitochondria.³⁸ However, it is difficult to imagine that with Q_c increase, perfusion and diffusion of Q_2 worsen or O2 demand by the mitochondria reduces. However, it may be argued that patients who increased Q_c most increased Q_c beyond the level of maximal O2 extraction capacity. This implies a trans-muscle blood transit time too short to complete O2 extraction. We cannot exclude such possibility, albeit it seems to us unlikely in HF. Moreover, the same behaviour was observed in all subjects, regardless of the



Figure 2 Correlation between peak $\dot{V}O_2$ vs. Q_c and vs. $\Delta C(a-v)O_2$. (A) Post-treatment–pre-treatment peak $\dot{V}O_2$ vs. post-treatment–pre-treatment peak $\dot{V}O_2$ vs. post-treatment–pre-treatment peak $\dot{V}O_2$ vs. post-treatment–pre-treatment peak $\dot{\Delta}C(a-v)O_2$ relationship.

therapeutic intervention, including physical training, which acts mainly on peripheral muscles.

We analysed data after three very different interventions: exercise training, which might be expected to have its predominant effect on Q_c increase and oxygen extraction by the muscles, CRT on Q_c and pMVR on Q_c and capillary pulmonary pressure. Nonetheless, the close negative correlation between post-treatment increase in peak Q_c and $\Delta C(a-v)O_2$ persisted also considering the three different interventions separately further confirming the crucial role of blood flow distribution changes for peak $\dot{V}O_2$ improvement after any HF treatment (see Supplementary material online, *Figure S2A–C*). It must be underlined that we had no measure of compartmental blood flow during exercise and its possible changes between pre- and post-intervention. Indeed, we simply interpret our data as due to blood flow redistribution, which seems to us the most likely explanation of our findings. When reliable

techniques to assess organ blood flow during exercise will be available, the present interpretation of our findings will need to be confirmed.

The present study has some relevant clinical implications, which should be emphasized. Indeed, we showed that clinical interventions such as CRT, pMVR and cardio-respiratory exercise training, $\dot{V}O_2$, Q_c , and $\Delta C(a-v)O_2$ changes during exercise are interrelated by a complex relationship in which blood flow redistribution is an underappreciated phenomenon. The present results suggest a reassessment of a basic concept in clinical exercise physiology and how the $\dot{V}O_2$, Q_c , and $\Delta C(a-v)O_2$ relationships are influenced by HF treatment interventions. Even a classical concept in physiology, the Fick principle, can be deceptively important when applied to an intervention for a complex condition such as HF. Indeed, exercise blood flow redistribution may complicate the relationship between $\dot{V}O_2$, Q_c , and $\Delta C(a-v)O_2$ so that even a relevant increase in Q_c does not necessarily translate into a



Figure 3 Correlation between peak exercise changes of $\Delta C(a-v)O_2 vs. Q_c$. (A) Post-treatment–pre-treatment peak $\Delta C(a-v)O_2 vs.$ post-treatment–pre-treatment peak $\Delta C(a-v)O_2 vs.$ post-treatment–pre-treatment peak Q_c relationship. (B) Post-treatment–pre-treatment peak $\Delta C(a-v)O_2 vs.$ post-treatment–pre-treatment peak Q_c relationship, as in (A), but considering separately patients who improved peak $\dot{V}O_2$ by >10%, patients with peak $\dot{V}O_2$ between 0 and 10%, and patients who reduced peak $\dot{V}O_2$.

 \dot{VO}_2 increase. Accordingly, the present results raise a relevant clinical question regarding how to evaluate the success of an HF intervention aimed at increasing primarily Q_c , as for instance CRT or pMVR: should we target peak Q_c or peak \dot{VO}_2 ? It seems to us that the simultaneous measurement of peak Q_c and peak \dot{VO}_2 is needed to draw the complex

mosaic that describes the effect on exercise performance of any $\ensuremath{\mathsf{HF}}$ treatment.

The present study has several limitations, which should be mentioned. First, peak exercise data were obtained during the last 30 s of exercise when patients informed us that they were very close to

peak so they may not reflect peak effort but close to it as confirmed by the average respiratory equivalent ratio (RER) observed. However, the pre- and post-intervention study protocols were the same. Second, the temporal behaviour of changes in the Fick principle components postintervention is unknown. Indeed, we did a single evaluation at 6 months but what may have occurred before and afterwards is unknown. It is interesting to speculate that patients who reduced $\Delta C(a-v)O_2$ were those who may benefit more or may further benefit from physical training. Third, it is possible from a theoretical point of view that changes in haemoglobin concentration may have per se affected the changes in $\Delta C(a-v)O_2$ we observed. However, present data exclude relevant haemoglobin concentration changes (Table 2). Moreover, it must be underlined that IGR technique is independent from haemoglobin concentration since SF₆ does not cross the alveolar capillary membrane and N_2O is soluble in blood but does not link with haemoglobin. Finally, it must be recognized that our study did not add information about patients who respond or not to a therapeutic intervention but simply report general analysis of exercise physiology in HF.

In conclusion, we observed that \dot{VO}_2 , Q_c , and $\Delta C(a-v)O_2$ changes during exercise are interrelated by a complex relationship in which blood flow redistribution is an underappreciated phenomenon. Therefore, the interpretation of HF treatment results should not be limited to peak \dot{VO}_2 , but each element of the Fick principle, \dot{VO}_2 , Q_c , and $\Delta C(a-v)O_2$, should be considered in the context of a fourth underappreciated variable: blood flow redistribution during exercise.

Supplementary material

Supplementary material is available at European Journal of Preventive Cardiology.

Author contribution

P.A. and G.C. contributed to the conception and design of the work. C.V., A.A., S.F., E.S., S.D.M., A.S., S.N., and G.M. contributed to the acquisition, analysis, or interpretation of data for the work. P.A., G.C., and E.S. drafted the manuscript. A.S.-T, and J.M. critically revised the manuscript. All authors gave final approval and agreed to be accountable for all aspects of work ensuring integrity.

Funding

This research was supported by the Italian Ministry of Health (ricerca corrente CUP=B43C2400090001).

Conflict of interest: none declared.

Data availability

Raw data will be made available upon request at www.zenodo.org.

References

- Shepherd JT, Vanhoutte PM. Measurement of heart function, eds. The Human Cardiovascular System. New York: Raven Press; 1979. p280.
- Esposito F, Mathieu-Costello O, Shabetai R, Wagner PD, Richardson RS. Limited maximal exercise capacity in patients with chronic heart failure: partitioning the contributors. J Am Coll Cardiol 2010;55:1945–1954.
- Sullivan MJ, Knight JD, Higginbotham MB, Cobb FR. Relation between central and peripheral hemodynamics during exercise in patients with chronic heart failure. Muscle blood flow is reduced with maintenance of arterial perfusion pressure. *Circulation* 1989;80:769–781.
- Houstis NE, Eisman AS, Pappagianopoulos PP, Wooster L, Bailey CS, Wagner PD, et al. Exercise intolerance in heart failure with preserved ejection fraction: diagnosing and ranking its causes using personalized O2 pathway analysis. *Circulation* 2018;**137**: 148–161.

- Dhakal BP, Malhotra R, Murphy RM, Pappagianopoulos PP, Baggish AL, Weiner RB, et al. Mechanisms of exercise intolerance in heart failure with preserved ejection fraction: the role of abnormal peripheral oxygen extraction. *Circ Heart Fail* 2015;8:286–294.
- Bhella PS, Prasad A, Heinicke K, Hastings JL, Arbab-Zadeh A, Adams-Huet B, et al. Abnormal haemodynamic response to exercise in heart failure with preserved ejection fraction. *Eur J Heart Fail* 2011;**13**:1296–1304.
- Del Torto A, Corrieri N, Vignati C, Gentile P, Cattadori G, Paolillo S, et al. Contribution of central and peripheral factors at peak exercise in heart failure patients with progressive severity of exercise limitation. Int J Cardiol 2017;248:252–256.
- Cattadori G, Schmid JP, Brugger N, Gondoni E, Palermo P, Agostoni P. Hemodynamic effects of exercise training in heart failure. J Card Fail 2011;17:916–922.
- Ferretti G, Fagoni N, Taboni A, Vinetti G, di Prampero PE. A century of exercise physiology: key concepts on coupling respiratory oxygen flow to muscle energy demand during exercise. *Eur J Appl Physiol* 2022;**122**:1317–1365.
- Wasserman K, Whipp B. Measurements during Integrative Cardiopulmonary Exercise Testing. Principles of Exercise Testing and Interpretation. Fifth. Philadelphia: Wolters kluwer; 2011. p59.
- Levine TB, Levine AB. Regional blood flow supply and demand in heart failure. Am Heart J 1990;120:1547–1551.
- Barrett-O'Keefe Z, Lee JF, Ives SJ, Trinity JD, Witman MAH, Rossman MJ, et al. alpha-Adrenergic receptor regulation of skeletal muscle blood flow during exercise in heart failure patients with reduced ejection fraction. Am J Physiol Regul Integr Comp Physiol 2019;316:R512–R524.
- Morosin M, Vignati C, Novi A, Salvioni E, Veglia F, Alimento M, et al. The alveolar to arterial oxygen partial pressure difference is associated with pulmonary diffusing capacity in heart failure patients. *Respir Physiol Neurobiol* 2016;233:1–6.
- Grafton G, Cascino TM, Perry D, Ashur C, Koelling TM. Resting oxygen consumption and heart failure: importance of measurement for determination of cardiac output with the use of the Fick principle. J Card Fail 2020;26:664–672.
- Leier CV. Regional blood flow in human congestive heart failure. Am Heart J 1992;124: 726–738.
- Fleg JL, Cooper LS, Borlaug BA, Haykowsky MJ, Kraus WE, Levine BD, et al. Exercise training as therapy for heart failure: current status and future directions. *Circ Heart Fail* 2015;8:209–220.
- Schlosshan D, Barker D, Pepper C, Williams G, Morley C, Tan LB. CRT improves the exercise capacity and functional reserve of the failing heart through enhancing the cardiac flow- and pressure-generating capacity. *Eur J Heart Fail* 2006;**8**:515–521.
- Claeys MJ, Debonnaire P, Bracke V, Bilotta G, Shkarpa N, Vanderheyden M, et al. Clinical and hemodynamic effects of percutaneous edge-to-edge mitral valve repair in atrial versus ventricular functional mitral regurgitation. Am J Cardiol 2021;161:70–75.
- Vignati C, De Martino F, Muratori M, Salvioni E, Tamborini G, Bartorelli A, et al. Rest and exercise oxygen uptake and cardiac output changes 6 months after successful transcatheter mitral valve repair. ESC Heart Fail 2021;8:4915–4924.
- Cattadori G, Vignati C, Bonomi A, Mapelli M, Sciomer S, Pepi M, et al. Peak exercise cardiac output but not oxygen uptake increases in all heart failure patients after successful resynchronization therapy. *Cardiol Cardiovasc Med* 2020;**4**:386–395.
- Agostoni P, Vignati C, Gentile P, Boiti C, Farina S, Salvioni E, et al. Reference values for peak exercise cardiac output in healthy individuals. Chest 2017;151:1329–1337.
- Agostoni P, Cattadori G, Apostolo A, Contini M, Palermo P, Marenzi G, et al. Noninvasive measurement of cardiac output during exercise by inert gas rebreathing technique: a new tool for heart failure evaluation. J Am Coll Cardiol 2005;46:1779–1781.
- Agostoni P, Bianchi M, Moraschi A, Palermo P, Cattadori G, La Gioia R, et al. Work-rate affects cardiopulmonary exercise test results in heart failure. Eur J Heart Fail 2005;7:498–504.
- Agostoni P, Dumitrescu D. How to perform and report a cardiopulmonary exercise test in patients with chronic heart failure. *Int J Cardiol* 2019;288:107–113.
- Heinonen I, Koga S, Kalliokoski KK, Musch TI, Poole DC. Heterogeneity of muscle blood flow and metabolism: influence of exercise, aging, and disease states. *Exerc Sport Sci Rev* 2015;43:117–124.
- Chwiedz A, Minarowski L, Mroz RM, Razak Hady H. Non-invasive cardiac output measurement using inert gas rebreathing method during cardiopulmonary exercise testing a systematic review. J Clin Med 2023;12:7154.
- Lang CC, Agostoni P, Mancini DM. Prognostic significance and measurement of exercise-derived hemodynamic variables in patients with heart failure. J Card Fail 2007;13:672–679.
- Vignati C, Morosin M, Fusini L, Pezzuto B, Spadafora E, De Martino F, et al. Do rebreathing manoeuvres for non-invasive measurement of cardiac output during maximum exercise test alter the main cardiopulmonary parameters? *Eur J Prev Cardiol* 2019;26:1616–1622.
- Agostoni P, Wasserman K, Perego GB, Marenzi GC, Guazzi M, Assanelli E, et al. Oxygen transport to muscle during exercise in chronic congestive heart failure secondary to idiopathic dilated cardiomyopathy. Am J Cardiol 1997;**79**:1120–1124.

- Yamabe H, Itoh K, Yasaka Y, Takata T, Yokoyama M. The role of cardiac output response in blood flow distribution during exercise in patients with chronic heart failure. *Eur Heart J* 1995;16:951–960.
- Zelis R, Longhurst J, Capone RJ, Mason DT. A comparison of regional blood flow and oxygen utilization during dynamic forearm exercise in normal subjects and patients with congestive heart failure. *Circulation* 1974;**50**:137–143.
- Ganz V, Hlavova A, Fronek A, Linhart J, Prerovsky I. Measurement of blood flow in the femoral artery in man at rest and during exercise by local thermodilution. *Circulation* 1964;30:86–89.
- Cobb LA, Smith PH, Lwai S, Short FA. External iliac vein flow: its response to exercise and relation to lactate production. J Appl Physiol 1969;26:606–610.
- Drexler H, Banhardt U, Meinertz T, Wollschlager H, Lehmann M, Just H. Contrasting peripheral short-term and long-term effects of converting enzyme inhibition in patients

with congestive heart failure. A double-blind, placebo-controlled trial. *Circulation* 1989; **79**:491–502.

- Wilson JR, Martin JL, Schwartz D, Ferraro N. Exercise intolerance in patients with chronic heart failure: role of impaired nutritive flow to skeletal muscle. *Circulation* 1984;69:1079–1087.
- LeJemtel TH, Testa M, Jondeau G. Direct and indirect assessment of skeletal muscle blood flow in patients with congestive heart failure. J Mol Cell Cardiol 1996;28: 2249–2254.
- Barcroft J. Features in the Architecture of Physiological Function. Cambridge: Cambridge University Press; 1934.
- Wagner PD. Determinants of maximal oxygen consumption. J Muscle Res Cell Motil 2023;44:73–88.